

# Automated ECG Analysis for Localizing Thrombus in Culprit Artery Using Rule Based Information Fuzzy Network

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## ABSTRACT

Cardio-vascular diseases are one of the foremost causes of mortality in today's world. The prognosis for cardio-vascular diseases is usually done by ECG signal, which is a simple 12-lead Electrocardiogram (ECG) that gives complete information about the function of the heart including the amplitude and time interval of P-QRS-T-U segment. This article recommends a novel approach to identify the location of thrombus in culprit artery using the Information Fuzzy Network (IFN). Information Fuzzy Network, being a supervised machine learning technique, takes known evidences based on rules to create a predicted classification model with thrombus location obtained from the vast input ECG data. These rules are well-defined procedures for selecting hypothesis that best fits a set of observations. Results illustrate that the recommended approach yields an accurateness of 92.30%. This novel approach is shown to be a viable ECG analysis approach for identifying the culprit artery and thus localizing the thrombus.

## KEYWORDS

Cardio-Vascular Diseases, ECG, Identification, Classification, Information Fuzzy Network.

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## I. INTRODUCTION

THE regular 12-lead Electrocardiogram (ECG) has been employed clinically for more than 100 years for finding heart diseases [1]. An ECG supervising system evaluates the ECG signals from leads incorporated in different anatomical locations of the body for evidences of ST elevation [2]. ST elevation and depression measurements from the leads are plotted in a graphical display arranged in relation to the anatomical points that are the basis of the lead signals [3]. Supervising ECG for ST segment variation is the only non-invasive procedure that facilitates the recognition and documentation of all episodes of Ischemia as replicated by ST segment changes [4].

Machine learning techniques are being increasingly adopted for automatic identification of blocks by analyzing ECG signals. Neuro-Fuzzy methods can be used to estimate the unknown noise, present in the Electrocardiogram signals [5]. Adaptive neural combined with the Fuzzy System, is used to construct a fuzzy predictor for ECG analysis. For this system, setting up parameters such as the number of Membership Functions (MF), training time period and learning algorithm are determined by the learning data [6]. Due to the altered form of ECG signals with several frequency noises and existence of several arrhythmic events in a cardiac rhythm, automated elucidation of abnormal ECG classification becomes a demanding task [7].

However, adequate Identification of Thrombus in the Culprit Artery (ITCA) in the patient before performing an angiogram is necessary for

successful surgical outcome. Before designing an automatic thrombus identification system, the characteristics and properties of ECG signal have to be studied with respect to the thrombus location. Due to a wide range of patients with Myocardial Infarction (MI), the characteristic of ECG signal may vary among patients with the same heart disorder. Hence the main objectives of this paper includes: 1. Differentiating Non-Ischemic cause of ST elevation from Ischemic cause 2. Localizing culprit vessels and its segments by ECG using ST elevation myocardial infarction. Judgment of accurate location of a lesion in the coronary artery by analyzing the ECG signal is important in a typical intensive care or operating room for decision-making and further treatment of the patient. The key idea of the proposed method is to identify the culprit artery and thrombus location by eliminating other chances or causes such as Tachycardia using ST elevation in myocardial disorder. For this purpose, this article proposes a novel classification method for detecting the block in coronary artery, based on traditional conditions and criteria [9]. These conditions depend on ST Elevation or depression voltage levels in different lead systems and time intervals between points. The main advantage of the proposed method is that the cardiologist can make a quick decision to take further clinical procedures and can act as an aid for the physician (who is not specialized in cardiology) in primary health care centers.

The basic outline of the proposed methodology for detection of thrombus is as follows: ECG signal from the database is fed to the Savitzky-Golay filter [8] for smoothing. The feature parameters required to classify are measured using Stockwell Transform (starting point, peak point, end point), Nearest- Neighbor Interpolation (time interval between points) and measurement of peak amplitude (peak amplitude). The design of the overall recommended methodology is

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presented in Fig. 1.

Stockwell Transform [37] is an improvisation and combination of Short-Time Fourier Transform (STFT) and wavelet transform. The main function of this method is to analyze time-frequency and this paper implements Stockwell transform for point identification in ECG signal to locate the starting point, peak point, and end point of the ECG signal. Further, Nearest-Neighbor Interpolation is used for interpolating functions of more than one variable that constructs original data within the series of distinct set of identified data points. Further, it is used for calculating the time interval between two identified points in the signal. Nearest-Neighbor Interpolation is followed by Peak Amplitude Measurement, which is used to calculate the mV range of the base to peak voltage level. Finally, the features identified in ECG signal are classified based on the traditional criteria [9] using the Information Fuzzy Network.

In summary the proposed method consists of five steps: (i) Discretization and point detection using Stockwell Transform, (ii) Feature identification based on Nearest-Neighbor Interpolation and peak amplitude measurement, (iii) Evaluation of association rules based on traditional criteria, (iv) Classification using Information Fuzzy Network and (v) Block detection.

The organization of the article is structured as follows: Section II presents some of the current research work done in the automated localization of thrombus by classification of ECG Signal. The proposed methodology is presented in section III. The empirical results and the performance assessment of the proposed method with other traditional methods are presented in section IV, followed by conclusions in section V.

## II. LITERATURE REVIEW

Identification of Myocardial Infarction (MI) and Ischemic beat is done on pre-processed ECG signal. Pre-processing includes removing of Baseline Wander (BW) and Noise. The basic method used for BW removal is the Butterworth filter in [10, 11] and the authors in [12] used cut-off frequency depending on heart beat for 3rd order Butterworth filter. In [13] 0.3Hz cut-off frequency and in [14] authors used a cut-off frequency of 0.5 Hz. In [15], BW was eliminated using the low frequencies derivative-based filter. On the other hand [16, 17] employed moving average filtering to eliminate the BW. Further studies proposed in [30] employed median filter to estimate BW. In [25], median filter was used to remove BW by taking the difference between the residue

component of Empirical Mode Decomposition (EMD) and Original signal. Discrete Wavelet Transform (DWT) has also been employed for BW elimination. Many techniques are employed in literature to lessen the noise in ECG signals. Low-pass filters are the simplest once. Authors in [15] applied low-pass filters to remove high frequency noise. Author in [8] used SG filter with order 5. While in [26] author used Butterworth filter without specifying frequency and order of the filter. Low-pass filtering is also been employed using moving average filters in [19, 26]. After pre-processing the ECG signals, feature extraction is done to find the MI and Ischemia.

The feature extraction method uses the amplitude, points, time interval, segments and frequencies of the ECG. The Fourier transform is the most important method in signal processing which signifies the quantity of the signal made up by each frequency. Similarly Wavelet Transform, Fourier Transform, Principal Component Analysis (PCA) and reconstructed phase space (RPS) theory can be used in feature extraction [47]. Features extraction from wavelet transform, wavelet db4 [31], db6 [30] and db9 [19] is also useful in the identification of MI. EMD is used for extraction of feature in [31]. Since EMD can decompose signal into different frequencies, only 2nd level component are used. However, the first level corresponds to noise.

In literature many methods have been employed for dimensionality reduction for MI detection. Forward Feature Selection (FFS) used in [32, 35] is computationally more efficient over simple filter based methods. 840 features composed of wavelet coefficients was reduced using Fuzzy rough feature selection in [44] using different level of wavelets. Particle Swarm Optimization (PSO) [32] and Bat algorithm [27] have been used in features selection. Machine learning algorithms like Random Forest and Lasso are also used in features selection. In [36], Multilayer Perceptron (MLP) eliminates irrelevant features for classification.

Selected features are used in majority of classification techniques as normal or MI/ischemia ECG signal. Thresholding method was widely used for ECG classification in [20, 22, 45, 28, 29]. Using K value as 5, KNN classifier was used in [18] to classify the signal using description found in [46]. Support Vector Machines (SVMs) have been widely used for classification of ischemia and MI with linear [17, 18, 24, 33], Radial Basis Function (RBF) [18, 21, 25, 35], polynomial [11] and exponential chi-squared kernel functions [11]. Review in [47] used artificial neural networks, fuzzy logic, rough set theory, decision trees, genetic and hybrid algorithms for classification of various heart

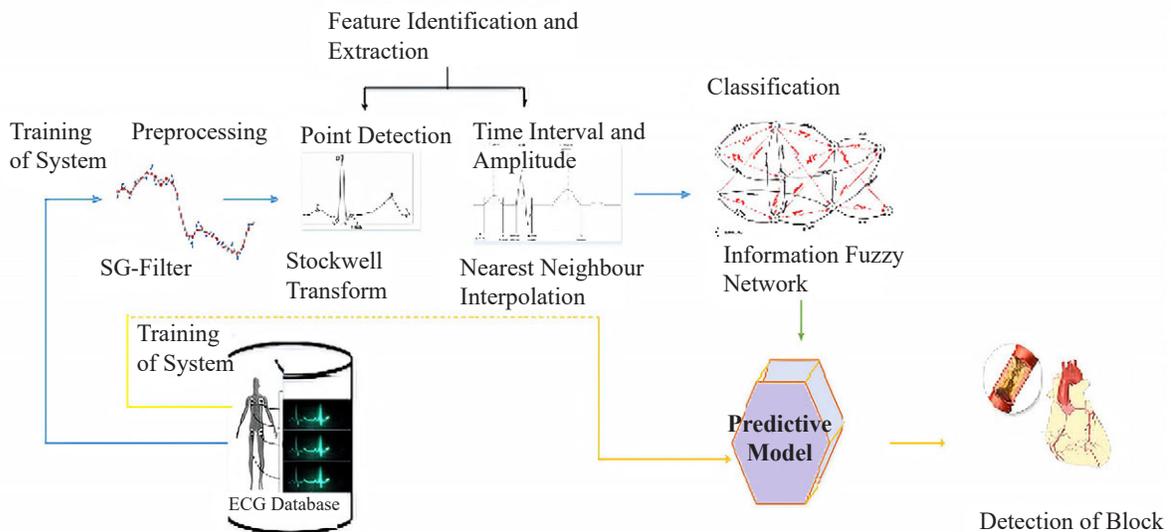


Fig. 1. Location of Thrombus in the Culprit Artery using Information Fuzzy Network.

diseases. Classifications based on Predictive Association Rules (CPAR) algorithm applied 6 association rules presented in [23] to classify ECG features. Expert knowledge is additionally been modelled with fuzzy logic in [5].

The vital role of a cardiologist is to take care of cardiac patients with utmost concerns. Thus computer aided feature extraction and analysis of ECG signals for disease identification has become a necessity. The initial step in Computer Aided Diagnosis (CAD) is the identification and extraction of the features of the ECG signals.

### III. RESEARCH METHODOLOGY

The first stage in developing an automated ECG classifier and thrombus location is to extract the characteristic features such as the points (P, Q, R, S, and T), time interval and amplitude from the waveform. Time interval and amplitude is considered as the first order and hence can be derived using Nearest-Neighbor Interpolation and Amplitude measurement technique. On the other hand, point detection can be obtained using Stockwell Transform. In a typical supervised classification scheme, the features are labeled with the decision outcome. Further, the IFN classifier is applied to the data through training and testing process.

#### A. Identification and Extraction of Time Interval and Amplitude

In the proposed methodology, classification of the ECG signal and identification of the culprit artery with the location of thrombus is fundamentally based on some of the features obtained from the ECG signal. The features that are identified and extracted are the point's identification (starting point, peak point, end point) of P, Q, R, S, T, time interval between points and peak amplitude. For point identification, an ECG signal has to be converted into its time-frequency distribution and frequency-dependent resolution, while preserving a direct relationship with time spectrum component. For this purpose, the Stockwell Transform [37], is used. The advantage of using Stockwell Transform is that it gives an accurate Time-Frequency representation and gives information about all points present in the signal. After identifying the ECG points, the necessary time interval between the points are calculated using Nearest-Neighbor Linear Interpolation method. It performs linear polynomials to construct original data points within the series of distinct set of identified data points. Finally, the amplitude of the ECG points such as R peak amplitude and ST segment amplitude is calculated by implementing Amplitude Measurement technique [38], which uses uneven threshold process to identify the R-peak and ST segment amplitude.

#### B. Stockwell Transform

The Stockwell Transform provides a frequency dependant resolution spectrum. The advantage of this transform is that it maintains a straight association with the Fourier spectrum. In this work, the advantages of Stockwell Transform to identify the ECG points are exploited. Stockwell Transform is equivalent to applying several Short-Time Fourier Transform (STFT) with different sized windows. It can be examined as a frequency dependent STFT or a phase corrected wavelet transform. In addition, it permits accessing any frequency component in the time-frequency domain.

Once the start point, peak point and end point of p wave, QRS complex, ST segment and T wave are detected from each lead, there is a need to calculate the time interval between every point. Each point in an ECG signal is located with respect to its value of amplitude or voltage in Y-axis and time value in X-axis. Earlier, scaled ECG papers were used to represent the ECG signal, where each unit box represented 40 milliseconds of time on the x-axis and 0.1 mv on the y-axis. During digitalization, the analog signal is converted into digital, which is

mapped on to a scaled function similar to that of the scaled ECG paper to identify the points present in the ECG. Further we implemented the Nearest-Neighbor Interpolation method to calculate the time interval between points.

#### C. Nearest-Neighbor Interpolation

A normal ECG signal composes of P wave, which is less than 0.25mV in amplitude and less than 0.12 sec in width. Q wave is less than 0.04 sec in duration and less than 25% of R wave, where R wave has amplitude of at least 0.5 mV in limb leads and 1mV in pericardial leads. The S wave amplitude is greater than R wave in lead V1 and smaller than R wave in lead V6. T wave does not exceed 0.5 mV in limb leads and it is 1 mV in pericardial leads. Also, normal PR interval ranges between 0.12 and 0.20 sec, QRS duration ranges between 0.07 to 0.10 sec, QT interval ranges between 0.33 to 0.43 sec and ST interval is 0.30 to 0.34 sec. In order to identify the points in the ECG we make use of the Nearest-Neighbor interpolation. By definition, Nearest-Neighbor interpolation is a process of determining approximate values of a function within a range bounded by two function values. In ECG signal analysis, once the points are detected, the interval between these points is determined using the Nearest-Neighbor interpolation method.

In this research work, we adopted a variable threshold method for peak amplitude measurement. We need to measure the amplitude of each segment, particularly R point and the peak of ST segment with J point. Since, we know the amplitude of every point on normal ECG signal, P wave which is less than 0.25mV, Q wave has amplitude of 0.30 -mV, R wave has amplitude of 1.5 mV, S wave has amplitude of 0.40 -mV and T wave does not exceed 0.5 mV. An amplitude threshold is determined as a fraction of the largest positive valued factor of that array. The threshold is fixed by defining  $d_{th}$  for each ECG signal, which is calculated using the following equation,

$$d_{th} = \frac{1}{2}((0.5 \times \max(\text{point}[q]) + \text{mean}(\text{point}[q]))) \quad (1)$$

The peak amplitude measurement is greatly affected by baseline wandering, which is the instability of the base line or change in isoelectric line position, which is likely to be moving up or down. This is primarily caused by improper connections in the ECG leads. Filtering the baseline can reduce wandering, thereby increasing the accuracy of amplitude measurement.

Fig. 2 shows all the features extracted (amplitude and time interval of each wave (P, Q, R, S, T, and U)) as required for classification and block localization in the culprit artery.

P wave threshold is 0.20 mV, Q wave threshold is -0.15 mV, R wave threshold is 0.9 mV, S wave threshold is -0.40 mV and T wave does not exceed 0.5 mV. When the peak is above the threshold, it is detected successfully. The entire feature identification and extraction process is presented in Fig. 2. Classification of ECG signal for locating block in the culprit artery is the next stage and it is presented in the next section.

#### D. Classification of ECG Signal

Several techniques for detecting blocks in coronary artery using ST segment in ECG signals have been analyzed. At present, medical equipment can vigilant a physician to the probable changes in ST and T wave deviations. But a specialist must still inspect these changes to decide whether they are due to blockage or not. Present methods of automatic classification for location of blocks are time-consuming and cannot discover blocks in real-time. This motivates a need for a capable system for automatic block detection. ECG Signal classification based on Information Fuzzy Network (INF) with rule based criteria distinguishes between different ECG signals that have different characteristics based on the extracted features analyzed earlier in this paper.

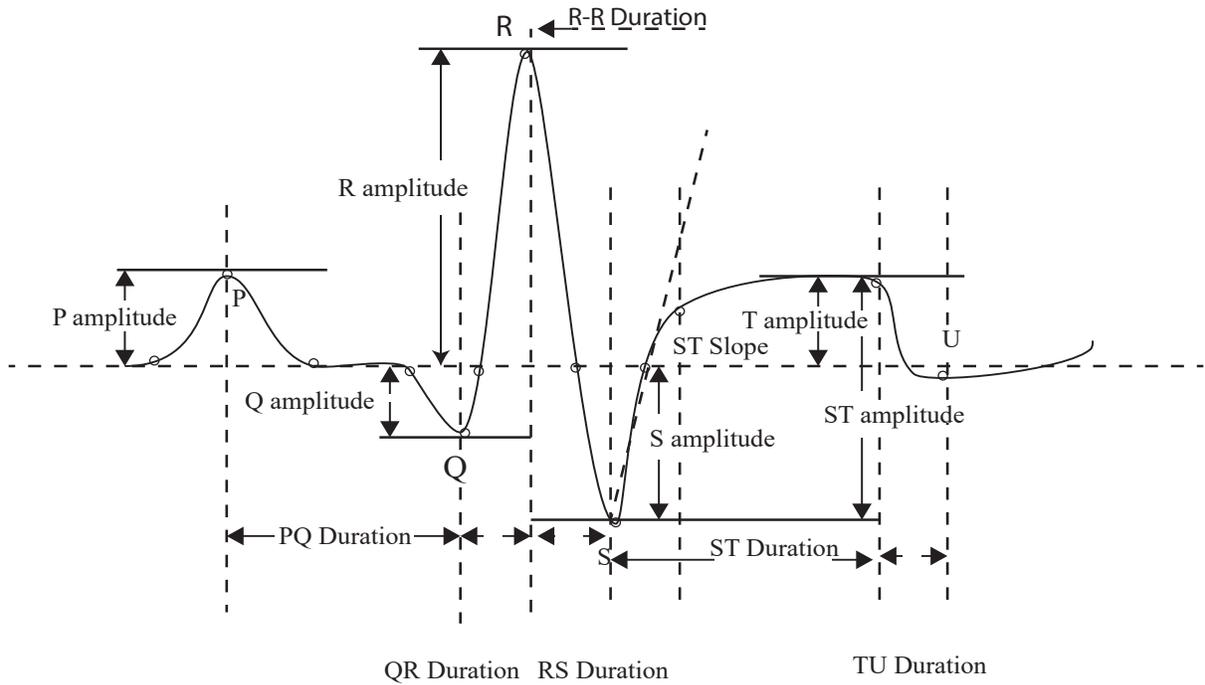


Fig.. 2. Extracted features from one ECG cycle.

### 1. Differentiating Ischemia and Non-Ischemic ECG Signals

An easy to-use, simple and accurate classification for locating the block has been proposed based on the evaluation of ST-segment changes in a 12-lead ECG that predicts the site of block in patients. There are several techniques employed for detecting Ischemia. However there are two methods which are widely used: coronary angiography and echocardiogram. While angiography is an invasive method for detection with 98% accuracy, echocardiogram is a non-invasive method with an accuracy of around 85%.

A block in the coronary artery causes variations in the depolarization of the heart's ventricular tissue. If the cardiac tissue is Ischemic, it results in improper depolarization. This shows an improper variation in current pulse, which causes a depression in the T-Q segment and an elevation in the ST segment. ST deviation can be calculated by using equations (2), (3) and (4) as follows,

To find ST Depression,

$$PR\ point(i'j) = \frac{1}{2} \text{ceil}(Rloc(i,j) - (S_{off}(i,j) - Q_{on}(i,j))) \quad (2)$$

To find ST Elevation,

$$ST\ point(i,j) = \frac{1}{2} \text{ceil}(Tloc(i,j) - T_{off}(i,j) - T_{on}(i,j)) \quad (3)$$

To find ST Deviation,

$$ST\ Deviation(i,j) = \text{abs}(x(PR\ point(i,j),i) - x(ST\ point(i,j),i)) \quad (4)$$

Where ceil is the Ceiling Function, the least integer greater than or equal to  $x$  abs is the Absolute Value, indicating the distance of the point or number from the zero point; the value of  $T_{on}$  and  $S_{off}$  is the first offset of S signal and  $T_{on}$  is the first onset of T wave which separates ST segment. From peak detection, zero crossing point behind the peak is considered as onset and zero crossing point ahead of the peak is detected as offset.

The ST deviation thus obtained is divided by 100; a normal ST deviation would be less than 0.148. Ischemia is detected if the ST Deviation obtained is greater than 1 (these condition are fixed using

cardiologist input). We confirmed that the ST deviation is caused by a block in coronary artery and if the condition is false, the ST deviation may be due to Non-ischemic causes. The flowchart given in Fig. 3 illustrates the method of differentiating Ischemia and Non-Ischemia.

### 2. Rule based Criteria for identifying the Culprit Artery and Localizing the Thrombus

One of the main objectives of this article is to identify the culprit artery from Ischemic ECG signals and finally to locate the exact position of the block as proximal, middle or distal. For this purpose, the classification process depends on the conditions given by [39]. The conditions for predicting the culprit artery is obtained from practical cases in real time situations. However, the main issue with this is the fact that the conditions are derived from independent leads. To overcome this problem, we adopted an ECG lead selector for analyzing the corresponding lead. The major conditions for identifying the culprit artery are thus: if ST elevation in leads L2, L3, aVF (limb lead), and L2 elevations are greater than L3 elevation, it is detected as Left Circumflex Artery (LCx). If L3 elevation is greater than L2 elevation, then it is detected as Right Coronary Artery (RCA). One more condition for RCA is that the V1 lead (Chest lead) must be greater than the V3 lead. Similarly, if V3 elevation is greater than the V1 lead, then it is predicted as the Left Anterior Descending Artery (LAD).

Further identifying the culprit artery, the exact spot of the block needs to be localized. Since identification in LAD is the lengthiest process as compared to the other branches, locating the block in LAD is valuable. Hence LAD is considered for locating the block. The primary condition is the presence of ST deviation in the lead aVF, L2 and L3, it is then predicted as the Proximal to major septal artery LAD. The next condition is the ST elevation in L1, avl, V5, V6 and it is then a proximal to major diagonal artery of LAD. Similarly if ST elevation is in L2, L3 and aVF, then it is distal to major septal artery of LAD. Finally ST elevation in V2, V3, and V4 with Right Bundle Branch Block (RBBB) is predicted as Proximal LAD. The remaining sub conditions for identification and localization are depicted in Fig. 4 and Fig. 5.

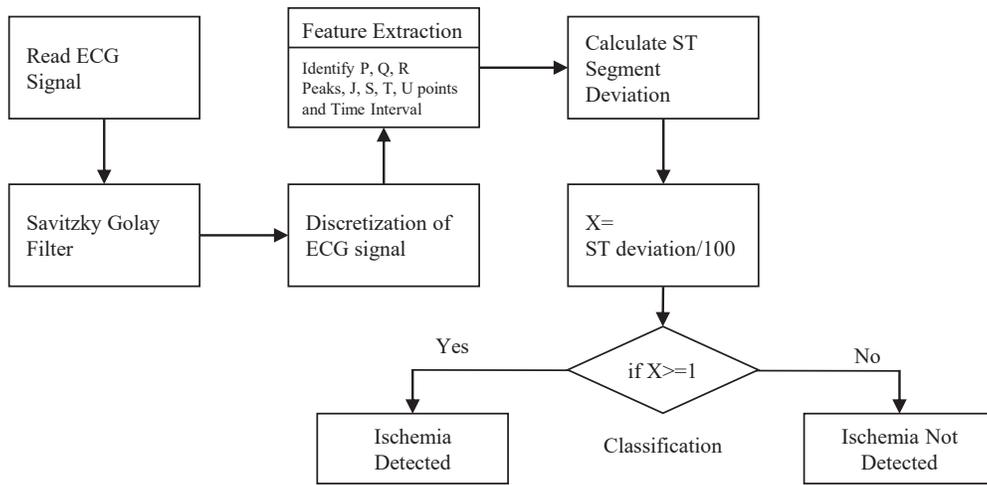


Fig. 3. Flow chart for differentiating Ischemia and Non-Ischemic.

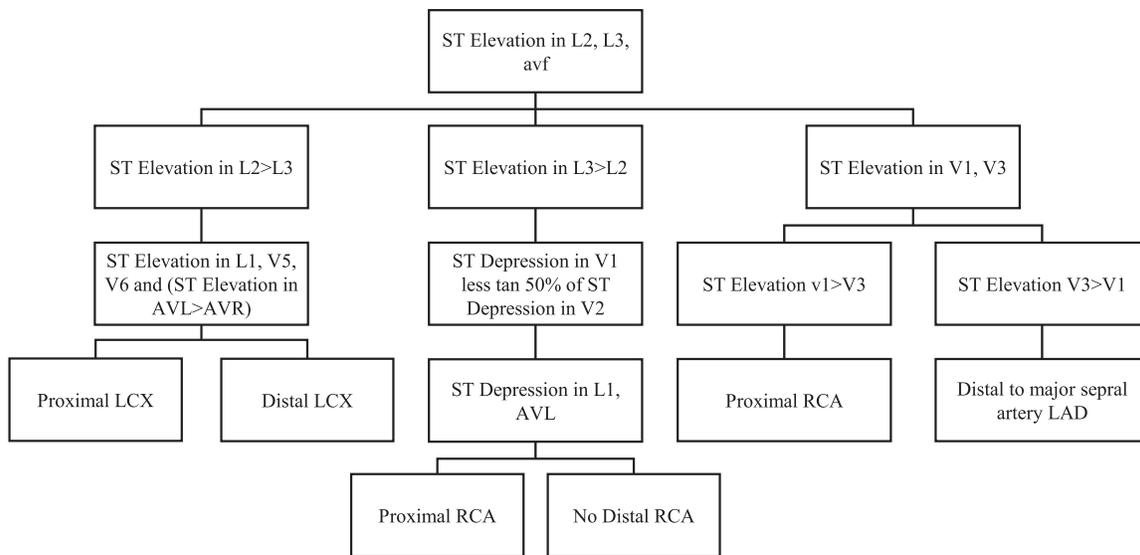


Fig. 4. Flow chart to identify the Culprit Artery.

### E. Information Fuzzy Network for ECG Classification and Identification of Block

The proposed approach for ECG classification and block location is based on the Information-Fuzzy Network (IFN). The IFN produces a ranked list of outputs relevant to a given set of input features as a result of inducing a correct classification task. Fig. 6 shows the model of the information fuzzy network.

IFN is a greedy machine-learning algorithm for supervised learning. IFN consists of many nodes. Every node inside the net is called as the inner or hidden node. Each node is weighted with conditional mutual information. IFN uses the conditional information in order to classify features during the identification stage. The set of nodes in the column are called layers, and each layer carries a condition for feature classification. However, there cannot be more than one condition in a layer. The IFN model is typically more stable, which means that small variations in the training set will affect it less, when compared to other models.

The whole classification process is made functional by imposing the previous conditions defined over the IFN. The root node is associated with the features that are extracted during the feature identification and extraction stage (such as amplitude and time interval). Each hidden layer consists of nodes representing equivalence classes of the

corresponding input variable. There are three hidden layers other than the root layer. Root layer is considered as the layer 0, while layer 1, layer 2 and layer 3 are the hidden layers and the target layer is the output layer. Layer 1 has the attributes or conditions for the Ischemic or Non-Ischemic causes. Layer 2 consists of two classes as shown in Fig. 6. The first class has the attributes or conditions for the classification of supraventricular from ventricular tachycardia, while the second class has the attributes or conditions for identifying the culprit artery. The IFN automatically determines the equivalence classes as contiguous sub-ranges of input values. Finally, the output layer has five output variables that indicate the location of the block in the culprit artery.

#### 1. Training IFN

A training set is a set of data employed to uncover the potentially predictive relationships between the input and the output. A test set is a set of data used to evaluate the strength and effectiveness of a prognostic association. Test and training sets are used in IFN, so that it can make predictions on new data. The accuracy and reliability of the block detection depends on the type of training set used. The database from MIT Physionet databank is divided into two splits: 30% of data to train and 70% to test the system.

Training phase is also called as weight updating or tuning phase

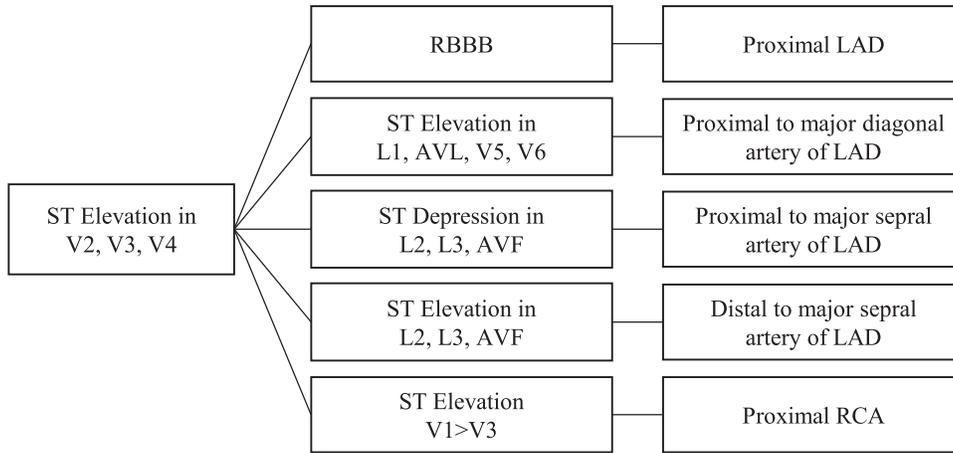


Fig. 5. Flow chart for localizing the Thrombus.

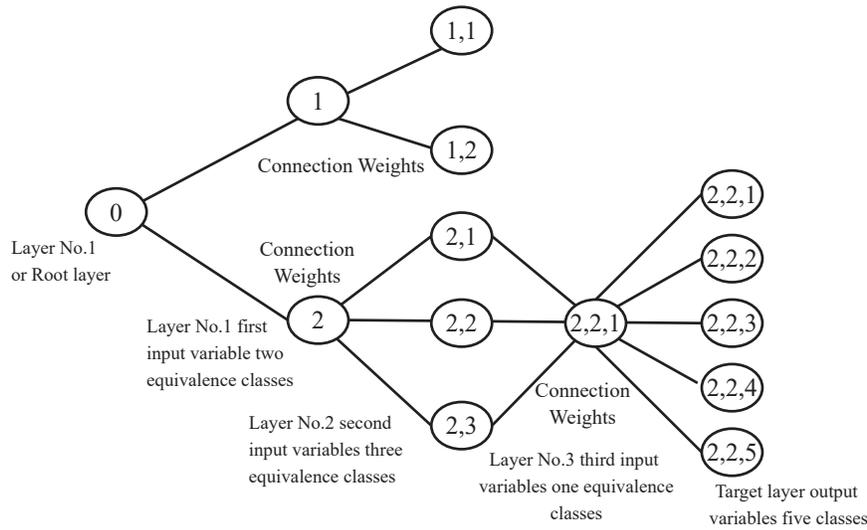


Fig. 6. IFN model for ECG classification and identification of block using Culprit Artery.

of the system. During training, the ECG signal from the database is applied to the system and the corresponding output is analyzed for error function. The objective of the training phase is to reduce the error function so that the result obtained from testing would be more accurate. The training error of the estimated conditional mutual information between an input attribute  $A_i$  and the target attribute  $B_i$  in training phase is evaluated by using the likelihood-ratio statistic. The likelihood-ratio test is a general-purpose technique for testing the null hypothesis  $H_0$ , that two random variables are statistically independent. This likelihood-ratio can be used to compute a p-value or compared to a critical value to decide whether to reject the null model in favor of the alternative model. The default significance level (p-value) used by the IFN algorithm is 0.1 %. Likelihood-ratio statistic is given by,

$$R^2(A_i; B_i / n) = 2 \cdot (\ln 2) \cdot E^*(n) \cdot MI(A_i; B_i / n) \quad (5)$$

In the above equation (5)  $E^*(n)$  is the number of cases correlated with the node  $n$ . After detecting the training phase error, it needs to be minimized by adjusting the weighted function of IFN. The weights are modified in proportion to their contribution to the error. Updating is done after each cycle using the conditional mutual information as mentioned in the learning section. It must be pointed out that the weights ( $W$ ) are adjusted to ensure that  $-0.1 \leq W \leq 0.1$  for each revised step, so that the chances of overshooting of the weights may be minimized, in the course of smoothly approaching a minimum error solution.

## 2. Testing IFN

Testing is done by computing the features over a new signal sample and choosing the class label corresponding to the IFN with the highest output. Subsequent to training, the recommended model encodes in its weights information regarding class discrimination in the feature space called label, which is the desired Information Fuzzy Classifier. In the testing phase, the 70% of data is considered as input to the IFN model and its performance is evaluated. During the testing phase, the system labels the test vector in the dimensional space. The output layer yields values by indicating the training pattern in the corresponding output classes. Once the Information Fuzzy Network identifies the input-output relationships, testing consists of generating the test cases that represent the union of combinatorial tests for input variables included in the IFN model at each single output. The results drawn from the proposed methodology are given in the next section.

## IV. RESULTS

In this section, we present the results using the Information Fuzzy Network approach for automated block detection in the culprit artery. We perform an automated input-output analysis by training the Information Fuzzy Network. The proposed method is implemented using Intel i5 environment over a Personal Computer with 2.99 GHz CPU and 8GB RAM running on Windows 7 OS. The induced information fuzzy models are utilized for block detection. We evaluate

the performance of the proposed method by comparing Sensitivity, Specificity, Positive Predictive Value and Negative Predictive Value and Classification Accuracy as evaluation metrics.

### A. ECG Database

In general, classifiers with a higher number of output classes require more features, which imply the need for a larger database. However, to prevent over-training, which would mean great performance on the training set, but a poor performance in testing sets, the database considered represents a well-defined differentiating feature set. Hence, we selectively combined some of the databases including ECG signals of patient with Ischemic Myocardial Infarction, Ventricular Tachycardia, Supraventricular Tachycardia and ECG signal of normal patient. The proposed methodology is implemented using MATLAB R2013a platform, and the experimental results are analyzed and compared with the conventional methods. The data chosen from MIT Physionet databank for training and testing are: Long-Term ST Database, consisting of 86 records that are 21 to 24 hours long, and contain two or three ECG signals, annotated beat-by-beat. With respect to the ST episodes as the rhythm changes, the signal quality changes. Each record includes ST level time series based on 16-second averages centred on each beat. Spontaneous Ventricular Tachyarrhythmia Database contains 135 pairs of RR interval time series, recorded by implanted cardioverter defibrillators in 78 subjects. Each series contains between 986 and 1022 RR intervals. One series of each pair includes a spontaneous episode of Ventricular Tachycardia (VT) or Ventricular Fibrillation (VF) and the other is a sample of the intrinsic (usually sinus) rhythm. T-Wave Alternans Challenge Database contains 100, 2, 3, and 12-lead ECG records sampled at 500 Hz with 16-bit resolution over a  $\pm 32$  mV range, including subjects with risk factors of sudden cardiac death as well as healthy controls and synthetic cases with calibrated amounts of T-wave Alternans [37]. The output ECG signals and results are illustrated in Fig. 7(a). Fig. 7(a) shows the original ECG signal from database and Fig. 7 (b) shows the filtered ECG signal using Savitzky-Golay filter.

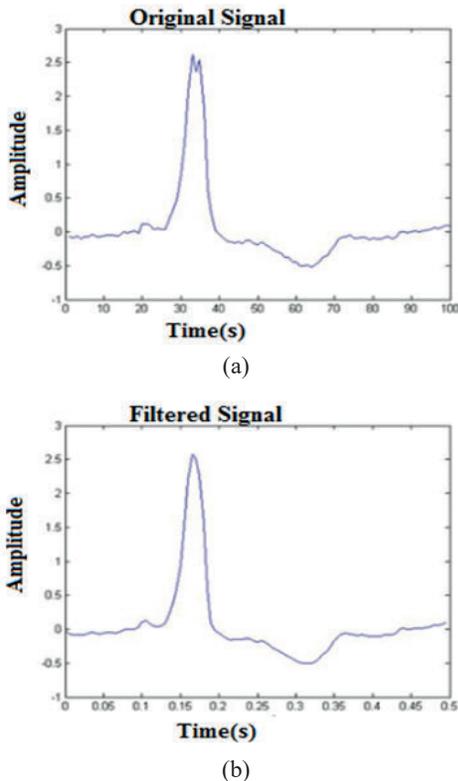


Fig. 7. (a) Original ECG signal (b) Filtered ECG signal using Savitzky-Golay filter.

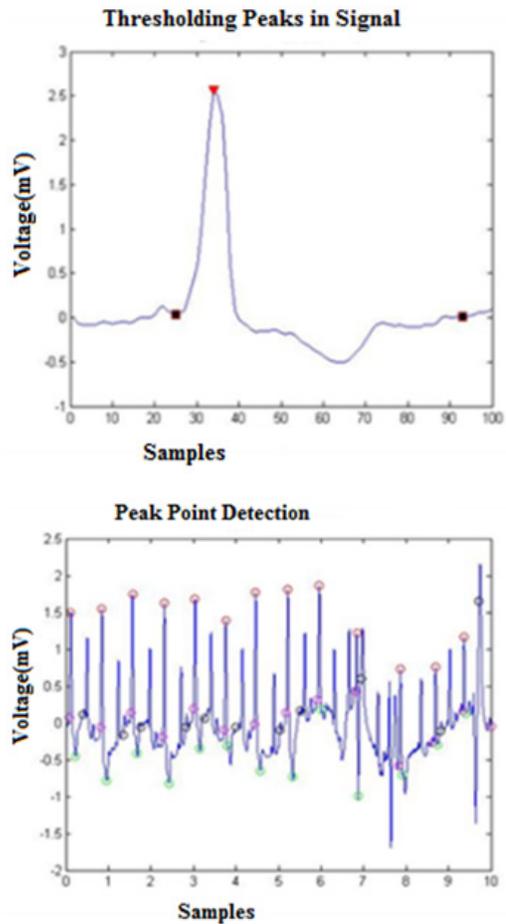


Fig. 8. Detection of points in ECG signal.

The original ECG signal shown in Fig. 7(a) is given as the input signal to the Savitzky-Golay filter. The output from the filter is further used for feature extraction process. The detection of points in the ECG signal is shown in Fig. 8. This figure shows the point detection by Stockwell transform. The extracted features such as time interval and amplitude of each point on ECG are tabulated in table I.

TABLE I. TIME INTERVAL AND AMPLITUDE OF ECG SEGMENT

ECG Segments	Time Interval (ms)	ECG points	Amplitude (mV)
RS segment	0.06271	S	0.4590
RR segment	0.14988	T	0.4090
ST segment	0.35	Q	0.3490

Table I shows the time interval of RS segment, RR segment and ST segment and the amplitude of the ECG Signal. In order to prove the efficiency and accuracy of the proposed method, the analytical performance of the proposed block detection using IFN approach is validated by the metrics given in the next section.

### B. Performance Evaluation

Performance evaluation is carried out by comparing classification accuracy of the proposed methodology with existing classifiers such as Support Vector Machine [40], Compound Neural Network [41] and Rough-Set-Based Inference Engine [42, 43] for ECG classification with five parameters: Sensitivity, Specificity, Positive Predictive Value (PPV), Negative Predictive Value (NPV) and Classification Accuracy.

The five performance parameters described above depicts the performance of the proposed methodology in terms of classification

of ECG signal and the detection of the block. The result shows the effectiveness of the system performance (see Table II). The efficiency of the proposed method can be well shown with the aid of comparative analysis. A comparison of the proposed method with other existing methods is given in the next section.

TABLE II. PERFORMANCE EVALUATION OF THE PROPOSED METHOD

Performance Parameters	Proposed Thrombus Detection using Information Fuzzy Network (IFN)
Sensitivity	87.50%
Specificity	100%
PPV	100%
NPV	83.33%
Classification Accuracy	92.30%

### C. Performance Comparisons

In this section, we compare the proposed method with Generalized Least Square-Support Vector Machine method, Compound Neural Network and Rough-Set-Based Inference Engine. In the first method, five types of ECG beats and the features from three transform approaches are independently classified using Least Square-Support Vector Machine (LS-SVM) [42]. The second method is based on a Compound Neural Network (CNN) to classify ECGs as normal or carrying an Atrio-Ventricular heart Block (AVB) [41]. This method uses three different feed forward multilayer neural networks. The third method is a rule-based rough-set decision system for the development of a disease inference engine [42], [43]. The proposed system is based on the criteria from popular medical literature and feedback from reputed cardiologists. All the performance evaluation metrics are used for the comparison are tabulated in table III.

TABLE III. COMPARISON OF THE PROPOSED METHOD WITH OTHER EXISTING METHODS

Performance Parameters	Generalized Least Square-Support Vector Machine [42]	Compound Neural Network [41]	Rough Set Based Inference Engine [42, 43]	Information Fuzzy Network (IFN) (Proposed Method)
Sensitivity	84.62	65.54	48.00	<b>87.50</b>
Specificity	83.33	92.25	96.00	<b>100</b>
PPV	81.48	63.47	85.30	<b>100</b>
NPV	86.21	92.09	91.70	<b>83.33</b>
Classification Accuracy	85.59	87.01	91.00	<b>92.30</b>

From Table III, it is clear that the ECG signal can be used as a reliable indicator for detecting heart blocks. In this research work, ECG analysis is effectively used as a non-invasive tool for the classification and location of the block in the coronary artery. Here, our proposed methodology was compared with Compound Neural Network, Rough Set based Interface Engine and Least Square-Support Vector Machine in terms of Sensitivity, Specificity, and Classification Accuracy. The obtained results proved a valid performance improvisation.

The proposed method for block detection in the culprit artery based on traditional conditions derived from real time incidents is presented. These conditions are formed as a generalized algorithm and implemented using Information Fuzzy Network. The results of the proposed method are tabulated in Table II and Table III. The results of the filtering method used are presented in Fig. 7. It shows the original ECG signal from the database and the filtered ECG signal. From Table III, it is clear that the proposed system is highly efficient, as the rate of Sensitivity is 87.5%, Specificity is 100% and Classification

Accuracy is 92.30%; which are more accurate as compared to other methods. Also, the rate of Positive Predictive Value is 100% and Negative Predictive Value is 83.33% and classified output is high when compared to other methods. Similarly, to prove the effectiveness of the proposed methodology, it has been compared with other conventional works that use different ECG classification to analyze ECG signal. The comparisons results presented in table 3 depicts that the results achieved by implementing the proposed method are far better than the works proposed earlier.

## V. CONCLUSION

In this research work, a method for identification of culprit artery along with detection of block location based on Information Fuzzy Network using ECG signals is developed. The decision of the proposed classification results are obtained from traditional criteria. The proposed detection system is validated successfully with 264 ECG samples with ST episodes variation, RR interval time series variation and T-Wave Alternant signals from both genders and different ages. The proposed method first distinguishes the ECG signals as Ischemic or Non-Ischemic, identifies the culprit artery and finally locates the block in the identified artery. The proposed detection system achieves 92.30% of accuracy. All the input voltage parameters and the output of the logical expressions related to the proposed detection criteria are expressed in the IFN system.

In future, we are intended to apply deep networks which could further enhance the results of the proposed method. It is also possible to employ various other soft computing techniques to find the percentage of blockage in the culprit artery.

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